

## Binary Titanium-Zirconium Alloy for Surgical Implants as well as Production Process Thereof

### Field of the Invention

The present invention relates to an alloy of titanium (Ti) and zirconium (Zr) for the production of surgical implants. A first application includes, for example, screws, plates and pins for fracture treatment and surgical orthopedics as well as endoprostheses. A second application includes dental surgery with in-bone implants, abutments and elements for suprastructures. The alloy is furthermore suitable for implants to anchor prostheses in the facial area, e.g. for maxillofacial and extraoral implants. The invention furthermore relates to a process for the production of such an alloy.

### Background of the Invention and Prior Art

The metallic materials used today for surgical implants are:

- stainless steel in accordance with international standard ISO-Norm 5832-1;
- cobalt-chromium-molybdenum alloys in accordance with ISO 5832-4, 5832-5 and 5832-6;
- unalloyed titanium in accordance with ISO 5832-2;
- alloys: titanium-aluminum-vanadium (Ti6Al4V) in accordance with ISO 5832-3; titanium-aluminum-iron (Ti5Al2, 5Fe) in accordance with ISO 832-10; titanium-aluminum-niobium (Ti6Al7Nb) in accordance with ISO 5832-11.

[Missing text]... ability of a material to perform with appropriate host response in a specific situation" (cf. D.F. Williams: in Biomaterials: Proceedings of a Consensus Conference of the European Society for Biomaterials. Elsevier Science Publ. Amsterdam, 1989). The foreign body produces only a minimal reaction in the living tissue. In the tissue in contact with the metal, sequestration in the form of encapsulation without pathological cell forms, or inertia, detectable as loose connective tissue, is observed (cf. S.G. Steinemann: Corrosion of Titanium and Titanium Alloys for Surgical Implants. Titanium, Science and Technology, Proc. 5<sup>th</sup> Int. Conf. Titanium. [G. Lütjering, U. Zwicker, W. Bunk, eds.], Deutsche Ges. Metallk. Oberursel, 1985, 1373).

For dental implants that are anchored in the bone, a higher form of tissue compatibility, namely osseointegration, is effective. In P.-I. Branemark, G.A. Zarb. T. Albrektsson [editors]: Tissue-Integrated Prostheses, Quintessenz Publ. Chicago, 1985, p. 11, we read: "Osseointegration is defined as a direct structural and functional connection between ordered, living bone and the surface of a load-carrying implant." This reaction implies an interaction between the foreign body and the living tissue, that is, more than just inert behavior of the metal. Dental implants are produced from titanium. For this metal, animal tests have shown complete anchoring, namely a rigid connection against the effects of pressure, shear and tension (cf. S.G. Steinemann, F. Straumann: [Ankylotische Verankerung von Implantaten] Ankylosis Anchoring of Implants. Schweiz. Mschr. Zahnmed. 94, 1984, 682). Complete anchoring also means adhesion, which is attributed to chemisorption (cf. S.G. Steinemann, J. Eulenberger, P.-A. Mäusli, A. Schroeder: Adhesion of Bone to Titanium. Biological and Biomechanical Performance of

Biomaterials [P. Christel, A. Meunier, A.J.C. Lee, eds.], Elsevier Sci. Publ. Amsterdam, 1986, 409).

Implants of bone and dental surgery are subject to high stresses and must be mechanically strong. Important parameters are yield point, elongation at break and modulus of elasticity. Stainless steel and unalloyed titanium have low strength and are therefore cold worked. For titanium, this increases the tensile strength from approximately 500 MPa to approximately 700 MPa. However, the strength of the two standard titanium alloys, which ranges from 900 – 1000 MPa, is not reached.

One experiment for measuring osseointegration is the implant expulsion test. For this purpose, a cylindrical implant is inserted into the bone in animal tests and the expulsion force is determined as a function of the rest period, typically 12 weeks. Such experiments have shown that the anchoring of mechanically roughened unalloyed titanium, Ti6Al4V and Ti6Al7Nb, is equal in strength but that a mechanically roughened and chemically etched surface for pure titanium implants results in much higher expulsion forces than an identical surface treatment for alloy implants (cf. M. Wong, J. Eulenberger, R. Schenk, E. Hunziker: Effect of surface topology on the osseointegration of implant materials in trabecular bone. J. Biomed. Mater. Res. 29, 1995, 1569). One or all of the three alloyed elements Al, V, Nb obviously inhibits integration in the bone.

Pure titanium and titanium alloys may exhibit local corrosion in narrow crevices if exposed to hot chloride-containing electrolytes. Manuals specify temperatures above 70° C (cf. B. Craig: Technical Note Corrosion. in Material Properties Handbook: Titanium Alloys [R. Boyer, G. Welsch, E.W. Collings, eds.], ASM Int., Metals Park OH, 1994, 1065). However, there is clinical literature reporting corrosion in the crevice of cone connections of artificial hip joints and on the shaft of such prostheses in the cement bed. The known titanium materials for implants are obviously not resistant to crevice corrosion.

[Swiss Patent Application] CH-A-544 154 discloses a binary titanium-zirconium alloy with 25 – 75% by weight Zr for implants. The composition range corresponds to high mechanical strengths. These metals are reactive, exhibit exothermal oxidation and are therefore not easy to process. On the other hand, the alloy formula corresponds to an atom concentration of 15 – 61% Zr, i.e., the added element strongly influences electrochemical and biological reactions. This is not desirable and the reactions specific to titanium in the living tissue should not be lost.

#### Object of the Invention

In view of the current lack of an optimal alloy for the aforementioned applications, the object of the invention is to create a metallic biomaterial which, firstly, exhibits high strength, secondly, is tolerated and integrated in both soft and hard tissue and, thirdly, is resistant to crevice corrosion.

### Summary of the Invention

A binary alloy of titanium and zirconium is proposed, wherein the added zirconium component is less than 25% by weight (14.9 atomic %) but more than 5% by weight (2.7 atomic %) resulting in a titanium-rich alloy. Preferred ranges of the zirconium content are between 19% by weight and 10% by weight.

The characteristics of the production process of the alloy are that the alloy is hot forged and subsequently cold worked. The forging process is carried out at temperatures above 850° C with subsequent rapid cooling of the alloy. Alternatively, the forging process may be carried out in the range of alpha/beta phase transition at 770° C to 830° C to produce special microstructures.

Thanks to the invention, a metallic biomaterial is now available for the defined field of application, which has sufficient strength as well as excellent tissue compatibility in soft and hard tissue and is moreover resistant to crevice corrosion.

Description of Details

It is known that the mechanical properties of titanium are substantially enhanced by adding zirconium (cf. A.G. Ingram, D.N. Williams, H.R. Ogden: Tensile properties of binary titanium-zirconium and titanium-hafnium alloys. *J. Less-Common Metals* 4, 1962, 217). Our own measurements on five alloys are given in Table 1. The alloys were melted from technically pure metals and, in addition to Ti and Zr, contained 0.09 – 0.11% O and 0.02 – 0.03% N; their condition was “forged above alpha-beta transition and cooled.”

Composition % by wt. Zr	Tensile	Yield Point	Elongation	Stress at
	Strength MPa	MPa	at break %	break MPa
Ti + 5.1	496	429	23.1	1526
+ 9.9	555	503	18.1	1436
+ 14.9	655	559	14.5	1469
+ 19.9	748	728	10.9	1454
+ 25.6	779	670	8.5	1127

*Table 1*

It is not generally known that the binary titanium-zirconium alloy can be further hardened by cold working and/or by adding oxygen. The alloys according to the invention are also readily cold worked, e.g., by rolling. The following strength values in accordance with *Table 2* were measured on a Ti15Zr alloy that was annealed above the alpha-beta transition following hot forging:

Material Ti15Zr	Tensile strength	Yield point	Vickers Hardness kg/mm <sup>2</sup>
	MPa	MPa	
non cold worked	—	—	203
rolled 20%	769	704	259
40%	883	873	275
60%	944	937	309

*Table 2*

Oxygen must be considered a controlled alloy component that influences strength properties. Results are listed in *Table 3*.

Ti15Zr + Oxygen	Tensile strength	Yield point	Vickers Hardness [kg/mm <sup>2</sup> ]
	[MPa]	[MPa]	
0.1% O	655	559	203
0.2% O	780	670	240
0.3% O	864	735	267

*Table 3*

The mechanical properties of the known titanium metals used today are shown in *Table 4* (cf. ASM Metals Handbook 9<sup>th</sup> Edition, Vol. 3, Properties and Selection: Stainless Steels, Tool Materials and Special Purpose Metals. Amer. Soc. Metals, Metals Park OH, 1980, 353; S.G. Steinemann, P.-A. Mäusli, S. Szmukler-Moncler, M. Semlitsch, O. Pohler, H.-E. Hintermann, S.M. Perren: Beta-titanium alloy for surgical implants. Titanium 92 Science and Technology [F.H. Froes, I. Caplan, eds.], TMS Warrentale PA, 1993, 2689).

Material	Tensile Strength MPa	Yield Point MPa	Elongation at break %	Stress at break MPa
Ti Grade 2	450			
Grade 4	620	550	20.0	
Grade 4 cold worked	785	692	18.3	1095
Ti6Al4V	1076	940	14.7	1429
Ti6Al7Nb	1024	921	14.0	1400

*Table 4*

The stress at break (load at break/cross section at point of break) is a measure for the toughness of a metal. It is remarkably high for single phase Ti-Zr alloys and approximately equal to that of two phase (alpha-beta) alloys Ti6Al4V and Ti6Al7Nb. Tensile strength and yield point of the material according to the invention are also better than those of cold worked unalloyed Grade 4 titanium and nearly reach those of the alpha-beta alloys if the effect of cold working and oxygen addition is used. Incidentally, cold working and the addition of oxygen do not change in any way the tissue compatibility of the binary Ti-Zr alloy.

Cell cultures are a common test for determining the reactions in the presence of metallic foreign bodies. For soft and hard tissue, experiments with fibroblast and osteoblast cells are of interest. Three such experiments were conducted. Firstly, growing osteoblasts on an inert plastic base with the metal oxides being dissolved in the culture medium (concentration approximately micromolar, saturated), secondly, growing fibroblasts on metal in the culture medium and, thirdly, growing osteoblasts on metal in the culture medium. The following reactions were observed (see *Table 5*):

Test	Retardation	No retardation
Osteoblasts in dissolved metal salt		Al, Sn, Ti, Zr, Ta
Fibroblasts on metal	Cu, Mo, V	Ti, Nb, Zr, Ta
Osteoblasts on metal	Zn, Fe, Sn, Cu, Al, Mo, V, Ni, Ag, Nb, Ta	Ti, Zr

*Table 5*

No reaction of osteoblasts to the salts dissolved in the culture medium was found and the five metals tested also do not have a toxic effect in the implant test (see Steinemann, loc. cit., 1985). The result of the experiments with fibroblasts is the same as that of the implant test, where the four metals Ti, Nb, Zr and Ta exhibit inert behavior and Cu, Mo and V are toxic or cause sequestration. The result of the experiments with osteoblast cells that are in contact with the metal is clearly different; only Ti and Zr are inert. Growth of osteoblast cells and their unimpeded multiplication, however, is a prerequisite for both bone formation and osseointegration.

Adhesion of soft tissue and particularly also bone to the implant indicates a "bonding" reaction on an atomic scale between the organic and mineral materials and the metal. Organic materials are, for example, the amino acids as the building blocks of proteins and as the components of the so-called ground substance (organic component of bone). Calcium and phosphates are primary components of the bone mineral. One speaks of adsorption and chemisorption (short for chemical adsorption). It is known that amino acids are adsorbed to titanium oxide (anatase and rutile in powder form) and to zirconium oxide. It is also known that amino acids

are chemisorbed to titanium metal oxidized in air (cf. J.M. Gold, M. Schmidt, S.G. Steinemann: XPS study of amino acid adsorption to titanium surfaces. *Helv. Phys. Acta* 62, 1989, 246; J.M. Gold, M. Schmidt, S.G. Steinemann: XPS study of retrieved titanium and Ti alloy implants. Clinical Implant Materials [G. Heimke, U. Soltesz, A.J.C. Lee, eds.], Elsevier Sci. Publ. Amsterdam, 1990, 69). It is not known whether and how amino acids are adsorbed to zirconium and Ti-Zr alloys and in what form calcium and phosphorus occur. Experiments by means of photoelectron spectroscopy provided the following results shown in

*Table 6.*

Material	Amino acids	$\text{Ca}^{2+}$	$\text{H}_2\text{PO}_4^-$ and $\text{HPO}_4^{2-}$
Ti	++	++	++
Ti + 25 wt.-% Zr	+	+	+
+ 50 wt.-% Zr	+	-	+
Zr	+	-	+

*Table 6*

Legend:

- + adsorbed
- ++ strongly adsorbed
- no adsorption

Amino acids are chemisorbed. Calcium and phosphate bind to the oxidized metal in the form of surface complexes. The reactions are strong, particularly for Ti rich alloys, and they involve all three reactants of osseointegration. On the other hand, adsorption is lacking or is weaker for zirconium rich alloys.

Alloying with Zr also has the advantageous effect that it increases the corrosion resistance of Ti in chloride-containing electrolytes. This effect enhances resistance to crevice corrosion, but only if the Zr content does not exceed 5% by weight.

The concentration of 25% by weight Zr corresponds to a particle concentration of 14.9 atomic % or 1 Zr atom to approximately 7 alloy atoms. This ratio characterizes the titanium rich alloy. If the proportion is 1 Zr/12 atoms in the metal, corresponding to 8.3 atomic % (= 14.6% by weight), the alloy is said to be diluted and the titanium component then dominates with respect to the properties of the metal, particularly also with respect to compatibility and surface reactions. Thus, a preferred composition is the range of less than 19% by weight but more than 10% by weight zirconium. Particularly suitable for the purpose, then, is a metal with 14 – 15% by weight Zr.

This metal can be further hardened through cold working in accordance with the above figures. Strengths approaching 1000 MPa can then be reached, which approximates the properties of alpha-beta materials. The titanium alloy continues to include max. 0.30% by weight Fe, max. 0.05% by weight N, max. 0.10% by weight C and max. 0.015% by weight H as technical impurities. Depending on the production process (iodide or Kroll process), zirconium can contain 2 – 3% by weight hafnium, a non-toxic element. The alloy according to the invention may contain up to 0.5% by weight hafnium as impurity.